Optical coherence tomography (OCT) has revolutionised eye care and significantly improved our understanding of a number of retinal diseases.1 This non-invasive imaging technique utilises low-coherence interferometry to create cross-sectional images, measuring backscattered or back-reflected light. The first commercially available devices used time domain modality (TD-OCT) and were designed to visualise the retina at 10 µm resolution. They enabled us to obtain the first in vivo images of epiretinal membranes (ERMs), macular holes (MHS), macular oedema, drusen and other pathologies of the fovea.2–4

Further rapid development resulted in the higher resolution and greater speed of spectral domain OCT (SD-OCT). The new scanning speed of approximately 50,000 A-scans/second allowed SD-OCT to capture high-density 3D images of the structures of the eye. SD-OCT allowed us to reveal important clinical information in micro scale, as well as revealing the thickness of individual layers of the retina including the retinal nerve fibre layer (RNFL), retinal ganglion cell, plexiform, nuclear and photoreceptor layers by means of segmentation algorithms. The current commercially available SD-OCT devices use light wavelengths of 1,000–1,040 nm and how the new ability to penetrate below the RPE can improve our knowledge of choroidal morphology, in healthy and diseased eyes.

The choroid provides up to 70 % of blood and oxygen to the eye. Pathological changes of this vascular tissue may lead to malnutrition of the retina and therefore be involved in the pathogenesis of numerous retinal disorders. Swept source optical coherence tomography (SS-OCT) is a new development of a non-invasive imaging technique that uses a tunable laser source with a higher wavelength light than conventional spectral domain OCT (SD-OCT). This enables visualisation of tissues below the retinal pigment epithelium. Thanks to SS-OCT’s ultrahigh speed and ultrahigh resolution it is possible to assess choroidal layers as well as to automatically create 3D maps of its thickness and volume. This review is to discuss how SS-OCT has improved our understanding of choroidal anatomy and function in various retinal and chorioretinal diseases. In future, detailed evaluation of choroid may play a crucial role in the diagnosis and management of various retinal diseases.

Keywords
Swept source OCT, SS-OCT, AMD, macular hole, epiretinal membrane, central serous chorioretinopathy, vitreomacular traction syndrome

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The Choroid – What We Knew
Histopathological studies revealed that choroidal layers include the inner and outer Bruch’s membrane, the choriocapillaris, Sattler’s layer, Haller’s layer, delimited from the sclera by suprachoroidal layer (SCL) (lamina fusca, lamina suprachoridea). Quantitative and qualitative in vivo assessment of the choroid has interested retina specialists, since its role in various chorioretinal diseases was established. Ex vivo histological studies on the thickness of chorioretinal layers revealed the thickest tissue underlies the macula region, thinning of the choroid as a result of ageing and thickening in the course of different chorioretinal pathologies.0,12 Due to their poor resolution and repeatability, traditional imaging techniques, such as ultrasonography or magnetic resonance imaging, provide limited insight into the diagnostic possibilities of choroidal abnormalities.11,12 The analysis of choroidal vasculature by means of indocyanine green (ICG) angiography allows us to examine blood circulation, from the arteries to the veins.12 Nevertheless, we were unable to visualise specific layers and it was not possible to take precise thickness or volume measurements.

OCT in Choroidal Imaging
The first attempts at choroidal imaging were reported using SD-OCT devices. Richard Spaide made the first attempt to visualise choroidal
layers with commercially available SD-OCT systems by introducing enhanced depth imaging OCT (EDI-OCT). He discovered that an inverted image can be obtained by moving the device closer to the eye, positioning the choroid closer to the ‘zero delay line’, which enhances visualisation of tissues 500–800 µm below the RPE.

To improve the signal-to-noise ratio, 50 to 100 B-scans of the same location have to be created and averaged together. As a result, choroidal tissue can be assessed at several submacular points. This requires taking manual measurements with inbuilt digital calipers after an observer has identified the outer margin of the RPE and the choroid–sclera junction. The method proved to have high reproducibility using several commercially available SD-OCT devices, showing good inter-visit and inter-observer correlation of results.

3D analysis was proposed by some authors to evaluate choroidal thickness and choroidal volume. However, it involved time-consuming manual choroid segmentation and the information obtained is limited to the subfoveal area. Tian et al. presented an automatic segmentation algorithm for spectralis SD-OCT; however, it is not commercially available to the clinicians. Furthermore, choroidal thickness and/or volume maps cannot be created automatically.

Swept source OCT (SS-OCT) is a novel device that uses photodetectors instead of spectrometers or line cameras and employs a tunable frequency swept laser with a narrowband light source. Near infrared light of 1,050 nm wavelength is less vulnerable to light scattering, thus creating the potential to penetrate more deeply into tissue compared with conventional SD-OCT devices, which operate at around the 800 nm range. As a result, B-scans can be acquired much faster (100,000 A-scans/second compared with 50,000 A-scans/second in conventional SD-OCT) and higher resolution is achieved (1 µm versus 5–6 µm in SD-OCT). These improvements mean we can now obtain accurate 3D images of the retina and choroid and, for the first time, we are able to create choroidal thickness maps and automatically measure choroidal thickness. The device also provides a wider OCT scan of 12 µm versus 9 µm in conventional SD-OCT.

Choroidal SS-OCT Imaging in Healthy Eyes

The sharp, detailed images of what lies below the RPE enables us to distinguish the choroidal layers that are not visible when using conventional SD-OCT systems. The images correlate with histological findings: from the innermost Bruch’s membrane, choriocapillaris, Sattler’s layer (layer of medium-diameter blood vessels), Haller’s layer (outermost layer of the choroid consisting of larger-diameter blood vessels) and the outer choroidoscleral boundary (CSB) (see Figure 1A).

The inner edge of the choroid, Bruch’s membrane, is composed of the basal lamina of the RPE, collagen and elastic fibres. It compactly adjoins the choriocapillaris layer with no potential space or tissue between them.

The choroid’s outermost border will be further called the CSB. Some authors estimate this layer to be the innermost scleral layer, whilst others suggest it is the outermost choroidal layer. We observed that the CSB consists of two bands: the upper of which is hyperreflective; the lower of which is hyporeflective (see Figure 1B). When visualised by our group, this lower, hyporeflective band was judged to be the suprachoroidal space (SCS). Previously, this space had never been visualised in vivo in the macular area in a human eye without choroidal effusion. Short posterior ciliary arteries and vorticose veins penetrate through SCL.

Another significant improvement provided by commercially available SS-OCT is that automatic choroid thickness and volume measurements may be performed with excellent repeatability (see Figure 1C).

As different investigators have reported various mean choroidal thicknesses, ranging from 191 to 354 µm, further studies are required.

SS-OCT enables automatic choroidal volume measurement for the first time. Choroidal volume in the fovea is calculated as the volume of a 1,000 µm diameter cylinder, the base of which is the central area of the Early Treatment Diabetic Retinopathy Study (ETDRS) Grid. Central choroidal volume in SS-OCT was reported at 0.159–0.17 µm and was lower than that reported with SD-OCT.

In a normal population, choroidal thickness and volume has been negatively correlated with two independent variables: axial length and age. Correlation with refractive error is controversial, the literature reporting a ‘no’ to ‘weak’ positive correlation. Automated segmentation of choroidal measurements revealed for the first time that peripapillary and macular choroidal thickness and volume increase significantly after performing the water drinking test in healthy eyes.

SS-OCT in Retinal Diseases

Age-related Macular Degeneration

In developed countries, age-related macular degeneration (AMD) is one of the leading causes of reduced visual acuity for those aged 60 years or over. ICG angiography studies showed hypoperfusion in choroidal circulation in eyes with wet AMD. Although this suggests that choroidal function is altered in the course of this disease, the exact contribution of blood circulation in AMD pathogenesis is still being investigated.

Using Cirrus™ HD-OCT, Manjunath et al. confirmed choroidal thinning in eyes with dry AMD and further reduction in eyes with wet AMD compared with age-matched patients. He found no significant correlation between...
Figure 2: Swept Source OCT in Age-related Macular Degeneration

Choroidal thickness (white doublehead arrow) in dry age-related macular degeneration (AMD) (A) and in neovascular AMD (B, C). Suprachoroidal space is visible (A: red arrows; C: white and red arrows). It consists of two bands, the inner hyperreflective (black arrows), and the outer hyporeflective (red arrows), estimated to be suprachoroidal space.

Our observations are coincident with presented observations. Although we have reported an increase in the thickness of Sattler’s layer in early wet AMD (defined as the presence of soft drusen greater than 125 µm in diameter, pigment changes or drusenoid pigment epithelial detachment). Other authors also demonstrated a relationship between AMD severity and choroidal thickness reduction. Choroidal thinning was observed in patients treated with anti-VEGF agents.

Changes in choroidal thickness are not the only phenomenon noticed in AMD progression. Morphological analysis reveals the existence of an irregular CSB line in 25 % of eyes with dry AMD and in 50 % of eyes with wet AMD. Additionally, we noted CSB irregularities in all cases of wet AMD, which were qualified for management of anti-vascular endothelial growth factor (VEGF) (unpublished data).

We observed the SCL and SCS in 20 % of eyes with wet AMD and in 50 % of eyes with dry AMD.

Age-related Choroidal Atrophy

Age-related choroidal atrophy (ARCA) of tissue was first described by Spaide et al., who demonstrated that choroidal thinning was associated with choroidal small vessel loss in some non-myopic elderly patients. In ARCA, unlike in geographic atrophy and AMD, the RPE layer remains intact. Choroidal thickness observed with EDI-OCT was reported to be markedly decreased. AMD and ARCA affect older adults and may coexist. This suggests that ARCA may contribute to dry AMD pathogenesis. Future SS-OCT studies may enhance our understanding of ARCA and its implications.

Central Serous Chorioretinopathy

Central serous chorioretinopathy (CSCR) is characterised by serous detachment of neurosensory retina from the RPE. When Gass described CSCR in 1967, he proposed that it was the choriocapillaris hyperpermeability that was the source of the leak. Later, studies with ICG angiography and fluorescein angiography showed a generalised disruption of choroidal vasculature in eyes affected with CSCR, with diffuse hyperpermeability, confirming Gass’ original idea. EDI-OCT demonstrated very thick choroid in patients with CSCR (505 ± 124 µm). Further SS-OCT studies revealed that mean choroidal thickness was increased in classic, chronic and multifocal CSCR (see Figure 3), and was greater in areas with choroidal vascular hyperpermeability and in areas where punctate hyperfluorescent spots showed up on ICG angiography than in unaffected areas. Detailed SS-OCT analysis of 15 eyes with CSCR demonstrated focally enlarged vessels at the level of choriocapillaris in 53 % of cases, as well as focal or diffuse dilution in Sattler’s and Haller’s layers in all analysed eyes.

Choroidal thickening reportedly reduces following photodynamic therapy but not after laser photocoagulation. This suggests that laser treatment does not influence the underlying problem, which involves the choroid.

Interestingly, increased choroidal thickening was also reported in eyes after spontaneous CSCR resolution. We assume that hyperpermeability leads to both: choroid thickening and to CSCR recurrences. After the spontaneous resolution we can see thick choroid but there is no test to check vascular permeability. In our opinion this is an indirect proof of persistent vascular abnormalities in choroid. CSCR recurrences are frequent after spontaneous resolution of CSCR.

Vitreoretinal Interface Diseases

We recently analysed the morphology of outer choroidal margins in patients with different vitreoretinal disorders, including ERM, vitreomacular traction (VMT) syndrome and MH. Unlike in healthy eyes, an irregular outer CSB line, not following the natural shape of the eye wall, may be noted in different vitreoretinal interface diseases (see Figure 4). This is much more frequently observed in eyes qualified for surgery. For example, irregular CSB was observed in 25 % of eyes with ERM, but in 90 % of eyes with ERM qualified for surgery. These irregularities may reflect the activity of the process. Irregular CSB is also observed in 40–59 % of eyes with full-thickness MH and 60 % of eyes with lamellar MH. Additionally, the SCL and SCS were noted in 34 % of eyes with full-thickness MH, 44 % of MH fellow eyes, in 60 % of eyes with VMT syndrome and 19 % of eyes with ERMs. Progression in VMT syndrome may be more rapid than in full-thickness MH. ERMs are a ‘static’ disease: it was reported that patients lose one visual acuity line every 5 years. Further studies are required to investigate what role the degree of visibility of the SCL and SCS might play in ophthalmology.

An interesting finding in patients with ERM is that choroidal thickening is observed in the foveal area compared with normal age and refractive-error-matched subjects. We cannot exclude that increased thickness is associated with macular thickening, which results in higher oxygen and blood demand. Another hypothesis may be that choroidal thickening is primary to macular changes and causes retinal thickening. Choroidal thickness decreases after vitrectomy with ILM peeling in eyes with idiopathic ERM.
The role of the choroid in MHS is elusive. Some investigators reported reduced choroidal thickness in EDI-OCT studies of patients with full-thickness MH.52,53 This leads to the hypothesis that reduced vasculature, insufficient blood and oxygen supply, may increase the susceptibility of the fovea to traction.53 Subsequent EDI-OCT reports did not confirm choroidal thinning in patients with idiopathic MH.54

**SS-OCT in Glaucoma**

Glaucomatous neuropathy is one of the leading causes of blindness in the world. Histopathological findings in animals, cadavers and enucleated eyes suggest that axonal damage and subsequent retinal ganglion cells apoptosis are associated with lamina cribrosa (LC) thinning and deformation.54-56 It was demonstrated with EDI-OCT that LC in glaucoma patients is thinner than in normal subjects.57 However, the posterior lamina surface is not visualised clearly using this technique. 3D raster scanning with ideal sampling density in SS-OCT enables detailed analysis of the optic disc including LC. Focal LC defects, which corresponded with neuroretinal rim thinning and with visual field defects, were observed in glaucoma patients.58

Glaucoma affects choroidal thickness as well. Choroidal thinning was observed in overall, peripapillar and macular region in glaucoma patients compared with healthy controls.59

**Choroidal Imaging for Non-ophthalmological Conditions**

The choroid has the highest blood flow per unit weight of any tissue in the body. Being composed mainly of blood vessels, the choroid should be very vulnerable to vascular changes, such as prolonged vasospasm.

Tobacco smoke exposure has a vasoconstrictive effect on cerebral vasculature. Some authors demonstrated a decrease in the flow velocity of the ophthalmic artery, central retinal artery and posterior ciliary artery, suggesting a significant increase in vascular resistance.60,61 Therefore, the thinning of the choroid layer is an expected clinical outcome in chronic tobacco smoking. SD-OCT studies showed that the mean choroidal thickness at the fovea decreased significantly at 1 hour and at 3 hours following smoking.62 Sigler et al., in a multivariate analysis of variance, reported that a history of smoking was significantly associated with a thinner choroid in patients at all ages (mean CT: 148 ± 63 µm versus 181 ± 65 µm for non-smokers).63 Choroidal thinning was greater in smoking- than non-smoking early-AMD subjects. High positive correlation was reported between the pack-years of smoking and a thinner choroid (p<0.001).

Similar findings are suggested in migraine patients. Migraine is known to be a neurovascular disease, in which vasospasm occurs in the tissues outside the brain, especially in the retina layer, concurrent with a reduction in brain blood flow.64-66 Blood flow at the level of the central retinal artery and posterior ciliary artery is decreased, as was shown in colour Doppler ultrasonography.67 Recent SD-OCT studies confirm choroidal thinning in patients with migraine, which is greater in patients with aura than those without aura.68 Choroidal changes were followed by decrease in RNFL thickness in all patients. Moreover, thinning of the ganglion cell layer was reported in the group with aura.

The roles of hypoperfusion and ischaemic lesions have also been discussed in some neurodegenerative diseases. RNFL thinning was reported in Alzheimer’s disease, and Parkinson’s disease and multiple sclerosis.69-71 Retinal changes may be secondary to insufficient blood supply.

No analysis in SS modality has been performed on choroidal structure and thickness in mentioned situations associated with reduced choroidal blood flow. We believe that SS-OCT may contribute additional information how choroid changes with prolonged hypoperfusion.

The new possibility to examine tissues below the RPE in greater detail are of tremendous value and will likely become more widely utilised in neuro-ophthalmology and other fields where they can provide deeper insight into the pathogenesis, treatment and follow up of neurodegenerative diseases. OCT angiography with the use of higher wavelength in SS demonstrated recently reduced blood flow index in optic nerve head in patients with multiple sclerosis and further flow index reduction after optic neuritis.72 SS-OCT might provide more details on choroidal pathophysiology in the intercourse of neurodegenerative diseases.
Conclusion

Choroidal imaging marks a milestone in posterior segment OCT visualization. It not only provides quantitative evaluation of choroidal thickness and volume, but also makes qualitative assessment possible. For the first time, we can distinguish separate choroidal layers and discover new morphological characteristics of particular diseases. Now that this ultrahigh speed and ultrahigh resolution technology is commercially available, our diagnostic and monitoring abilities in choroidal diseases are better than ever. In the future, clinical application of SS-OCT may involve various neurological conditions as well as vitreoretinal pathologies.